

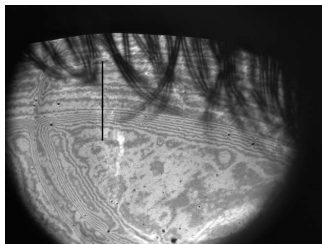
# Single-Equation Models for the Tear Film in a Blink Cycle with Realistic Lid Motion

A. Heryudono<sup>1</sup>, R.J. Braun<sup>1</sup>, T.A. Driscoll<sup>1</sup>, K.L. Maki<sup>1</sup>, L.P. Cook<sup>1</sup>,  
and P.E. King-Smith<sup>2</sup>

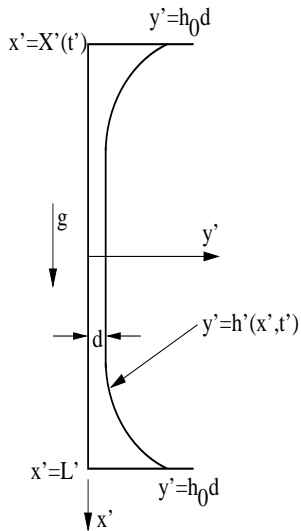
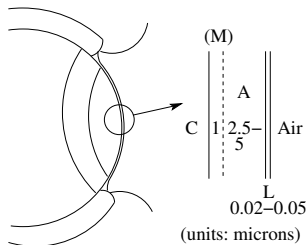
<sup>1</sup>Mathematical Sciences, U of Delaware  
and <sup>2</sup>College of Optometry, Ohio State U

APS DFD 2007 Meeting  
Salt Lake City  
November 18-20 2007

How do we simulate the dynamics of the tear film ?



Interference fringes.



$\epsilon = \frac{d}{L}$  is small  $\rightarrow$  Lubrication theory

## Physical parameters: Braun et al.

Constants	Description
$L' = 5 \text{ mm}$	half the width of the palpebral fissure ( $x$ direction)
$d = 5 \text{ }\mu\text{m}$	thickness of the tear film away from ends
$\epsilon = \frac{d}{L'} \approx 10^{-3}$	small parameter for lubrication theory
$U_m = 10\text{--}30 \text{ cm/s}$	maximum speed across the film
$L'/U_m = 0.05 \text{ s}$	time scale for real blink speeds
$\sigma_0 = 45 \text{ mN/m}$	surface tension
$\mu = 10^{-3} \text{ Pa}\cdot\text{s}$	viscosity
$\rho = 10^3 \text{ kg/m}^3$	density

- Inside the film

- Viscous incompressible parallel flow inside the film.
- Inertial terms and gravity are neglected.

- At the impermeable wall  $y = 0$

- $v = 0, \quad u = \beta u_y;$

- At the free surface  $y = h(x, t)$

- Simplified stress conditions

$$p = -Sh_{xx}, \quad S = \frac{\epsilon^3 \sigma}{\mu U_m}, \quad u^{(s)} = X_t \frac{1-x}{1-X}$$

- Kinematic condition

$$h_t + q_x = 0 \text{ on } X(t) \leq x \leq 1,$$

where

$$q = \int_0^h u(x, y, t) dy$$

- The uniform stretching limit (USL).

$$q(x, t) = \frac{h^3}{12} \left( 1 + \frac{3\beta}{h + \beta} \right) (Sh_{xxx}) + X_t \frac{1-x}{1-X} \frac{h}{2} \left( 1 + \frac{\beta}{h + \beta} \right)$$

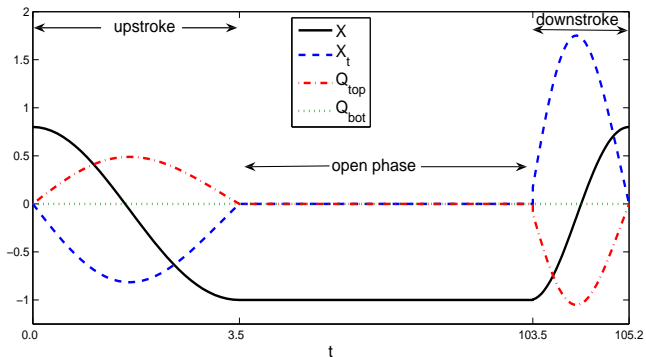
Boundary conditions

$$h(X(t), t) = h(1, t) = h_0 \quad q(X(t), t) = X_t h_0 + Q_{top} \quad q(1, t) = -Q_{bot}.$$

Initial condition

Polynomial function

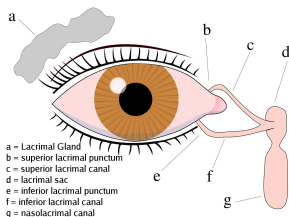
We depart from Berke and Mueller (98)  $\Rightarrow$  Heryudono et al (07)



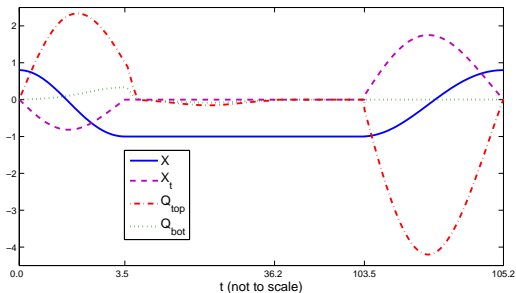
Flux proportional to lid motion (FPLM) (Jones et al (05))

$$Q_{top} = -X_t h_e, \quad Q_{bot} = 0$$

Add in lacrimal gland supply and **punctal drainage** approximated by Gaussians.



Picture above is taken from the Wikipedia commons



We transform the PDE into a fixed domain  $\xi \in [-1, 1]$  via

$$\xi = 1 - 2 \frac{1 - X}{1 - X(t)}.$$

The equations become

$$H_t = \frac{1 - \xi}{L - X} X_t H_\xi - \left( \frac{2}{L - X} \right) Q_\xi$$

$$Q = X_t \frac{1 - \xi}{2} \frac{H}{2} \left( 1 + \frac{\beta}{H + \beta} \right) + \frac{H^3}{12} \left( 1 + \frac{3\beta}{H + \beta} \right) \left[ S \left( \frac{2}{1 - X} \right)^3 H_{\xi\xi\xi} \right]$$

$$H(\pm 1, t) = h_0, \quad Q(-1, t) = X_t h_0 + Q_{top}, \quad Q(1, t) = -Q_{bot}, \quad (BCs)$$

$$H(\xi, 0) = h_m + (h_0 - h_m) \xi^m \quad (IC).$$

$\Rightarrow$  Spectral discretization in space and standard ODE in time.

- Use spectral collocation method.
  - Map Chebyshev points technique **Kosloff & Tal-Ezer (93)**
  - Use mapping parameter by **Don & Solomonoff (97)** to reduce roundoff errors near end points.
- Imposing boundary conditions.
  - Set Q

$$Q = X_t \frac{1-\xi}{2} \frac{H}{2} \left(1 + \frac{\beta}{H+\beta}\right) + \frac{H^3}{12} \left(1 + \frac{3\beta}{H+\beta}\right) \left[ S \left( \frac{2}{1-X} \right)^3 H_{\xi\xi\xi} \right]$$

- When computing  $Q_\xi$ , overwrite its end values with  $Q(-1, t) = X_t h_0 + Q_{top}$ ,  $Q(1, t) = -Q_{bot}$ .
- Solve the initial value problem at inner nodes.

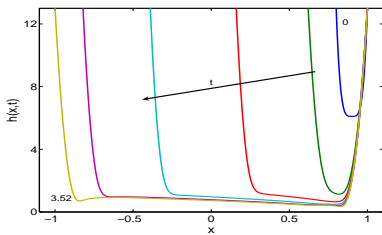
$$H_t = \frac{1-\xi}{1-X} X_t H_\xi - \left( \frac{2}{1-X} \right) Q_\xi$$

with ode solver ode15s.

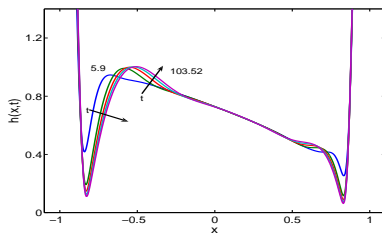


Parameters  $N = 351$ ,  $\lambda = 0.1$ ,  $\beta = 10^{-2}$ ,  $S = 2 \times 10^{-5}$ ,  $h_0 = 13$ ,  $h_e = 0.6$ , and initial volume  $V_0 = 2.576$ . Our simulation is done in MATLAB with ode15s as ODE solver.

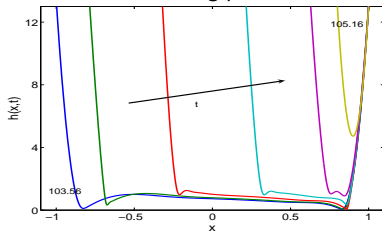
Opening phase

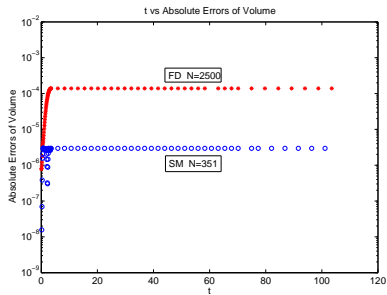
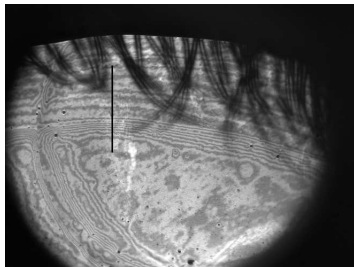
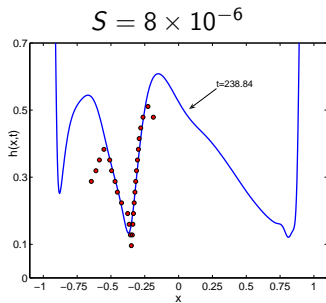
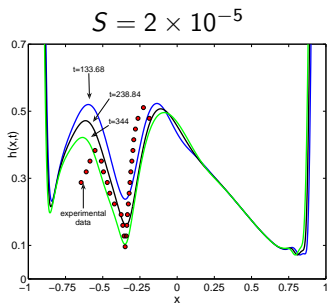


fully open (zoom)



The closing phase





Conservation of volume

## SUMMARY

- 1-D simulation of the tear film in a blink cycle.
- Good fit with experimental data for partial blink simulation with FPLM+ type fluxes.
- Use spectral methods for getting higher accuracy solutions.
- To appear in IMA Journal of Mathematical Medicine and Biology.